Intercellular Bridge Mediates Ca\textsuperscript{2+} Signals between Micropatterned Cells via IP\textsubscript{3} and Ca\textsuperscript{2+} Diffusion

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ABSTRACT Intercellular bridges are plasma continuities formed at the end of the cytokinesis process that facilitate intercellular mass transport between the two daughter cells. However, it remains largely unknown how the intercellular bridge mediates Ca\textsuperscript{2+} communication between postmitotic cells. In this work, we utilize BV-2 microglial cells planted on dumbbell-shaped micropatterned assemblies to resolve spatiotemporal characteristics of Ca\textsuperscript{2+} signal transfer over the intercellular bridges. With the use of such micropatterns, considerably longer and more regular intercellular bridges can be obtained than in conventional cell cultures. The initial Ca\textsuperscript{2+} signal is evoked by mechanical stimulation of one of the daughter cells. A considerable time delay is observed between the arrivals of passive Ca\textsuperscript{2+} diffusion and endogenous Ca\textsuperscript{2+} response in the intercellular-bridge-connected cell, indicating two different pathways of the Ca\textsuperscript{2+} communication. Extracellular Ca\textsuperscript{2+} and the paracrine pathway have practically no effect on the endogenous Ca\textsuperscript{2+} response, demonstrated by application of Ca\textsuperscript{2+}-free medium, exogenous ATP, and P2Y\textsubscript{13} receptor antagonist. In contrast, the endoplasmic reticulum Ca\textsuperscript{2+}-ATPase inhibitor thapsigargin and inositol trisphosphate (IP\textsubscript{3}) receptor blocker 2-aminoethyl diphenylborate significantly inhibit the endogenous Ca\textsuperscript{2+} increase, which signifies involvement of IP\textsubscript{3}-sensitive calcium store release. Notably, passive Ca\textsuperscript{2+} diffusion into the connected cell can clearly be detected when IP\textsubscript{3}-sensitive calcium store release is abolished by 2-aminoethyl diphenylborate. Those observations prove that both passive Ca\textsuperscript{2+} diffusion and IP\textsubscript{3}-mediated endogenous Ca\textsuperscript{2+} response contribute to the Ca\textsuperscript{2+} increase in intercellular-bridge-connected cells. Moreover, a simulation model agreed well with the experimental observations.

INTRODUCTION

In most cell types at the end of the cytokinesis process, one cell divides into two daughter cells with formation of a transient intercellular bridge that connects the cells before their final separation (1–3). The formation of the intercellular bridge is driven by several consecutive steps, including cleavage furrow ingression, constriction of an actomyosin-based contractile ring, creation and stabilization of a connective microtubular linkage, and its final abscission (4,5). The majority of studies in this field are focused on molecular events associated with formation and abscission of the intercellular bridge such as assemblage of endosomal sorting complex required for transport III (ESCRT-III) (6–9) and localization of testis-expressed gene 14 (10,11). Recently, it was found that the intercellular bridge in the early mouse embryo served as the microtubule-organizing center and coordinated the transport of cell adhesion molecules to the membrane (12) and that stable intercellular bridges in germline cells facilitated the sharing of messenger RNA (13), organelles (14), and other molecules (15). However, more important functions and physical characteristics of intercellular bridges still remain largely unknown.

SIGNIFICANCE It is well proven that intercellular bridges formed at the end of the cytokinesis process facilitate intercellular mass transport between the daughter cells. However, their role in the mediation of Ca\textsuperscript{2+}-based intercellular communication between postmitotic cells is still largely unknown. In this work, we utilize BV-2 microglial cells planted on specially designed micropatterned assemblies to resolve the spatiotemporal characteristics of Ca\textsuperscript{2+} communication over the intercellular bridge. We show that both passive Ca\textsuperscript{2+} diffusion and IP\textsubscript{3}-mediated endogenous Ca\textsuperscript{2+} response contribute to the signal transfer.
Ca\textsuperscript{2+} signaling is a principal form of cell-to-cell communication that coordinates the functions of a large group of cells and regulates various biological activities during growth and development (16–19). Ca\textsuperscript{2+} mobilization is triggered by the increase of cytoplasmic Ca\textsuperscript{2+} concentration in the initiating cell, which is subsequently followed by the increase of Ca\textsuperscript{2+} concentration in other cells. This process takes place either through the paracrine pathway in distant cells (20,21) or, in physically connected cells, through gap junction coupling (22,23).

Regular gap junctions enable spreading of Ca\textsuperscript{2+} signals either directly, by diffusion of Ca\textsuperscript{2+} ions, or indirectly, by diffusion of messenger molecules such as inositol triphosphate (IP3) (16,22,23). A recently discovered new type of cell-to-cell communication pathways, i.e., communication via tunneling nanotubes (TNTs) (24), was also reported to mediate the transmission of Ca\textsuperscript{2+} signals in multiple types of cells such as astrocytes (25), dendritic cells (26), and retinal pigment epithelial cells (27). As a physical continuity of the plasma between cells, TNTs represent a unique model to study Ca\textsuperscript{2+} signaling propagation in bounded narrow structures (28,29). Nevertheless, the instability and uncontrollability of TNTs restrict their suitability for advanced research on Ca\textsuperscript{2+} signaling.

In comparison to TNTs, intercellular bridges have larger width and exhibit better stability and controllability, which makes them an ideal system for quantitative analysis of Ca\textsuperscript{2+} signal propagation. In this work, we utilized BV-2 microglial cells to investigate the spatiotemporal characteristics of Ca\textsuperscript{2+} communication between postmitotic daughter cells via the intercellular bridge. The initial Ca\textsuperscript{2+} signal in one of the two daughter cells was provoked by a mechanical stimulus. A set of dumbbell-shaped micropatterned assemblies was used to regulate the length of the intercellular bridges formed during the cytokinesis. By this method, considerably longer and more regular intercellular bridges were obtained than in conventional cell cultures. A theoretical model mentioned above was used to simulate Ca\textsuperscript{2+} communication through the intercellular bridges, and very good agreement between experimental and computational results was found.

MATERIALS AND METHODS

Cell culture

The BV-2 microglial cells were routinely cultured in Dulbecco’s modified Eagle’s medium (Gibco, Gaithersburg, MD) containing 10% (v/v) fetal bovine serum (Biological Industries, Beit HaEmek, Israel), 100 U/mL penicillin, and 100 \( \mu \)g/mL streptomycin (Gibco) at 37°C under 5% CO\textsubscript{2}. Before being plated on glass coverslips, cells were isolated with 0.25% trypsin (Gibco) and diluted to a density of 3 \( \times \) 10\textsuperscript{4} cells/mL.

Substrate preparation

The micropatterned substrates were fabricated as previously reported (30). First, clean glass coverslips were placed into a hermetic flask containing hexamethyldisilazane (HMDS; Sigma-Aldrich, St. Louis, MO) vapor to enable deposition for 20 min. Then, a positive photoresist (RuiHong, Suzhou City, China) was spun cast on HMDS-covered substrates and photo-etched through a chrome-based photomask with designed patterns. After removing the exposed parts of the photoresist with a developing solution, the substrates were treated with oxygen plasma for 2 min and then dipped into anhydrous toluene containing 3 mM poly (ethylene glycol)-silane (Gel- est, Morrisville, PA) and 1% (v/v) triethylamine (Sigma-Aldrich) for 3 days to attain stable passivation. Next, to remove polyethylene glycol attached to HMDS regions, the substrates were successively sonicated in anhydrous toluene, ethanol, and deionized water. Then, fibrinectin (FN; Corning, Corning, NY) solution (150 \( \mu \)g/mL) in phosphate-buffered saline was spread over the substrates at 4°C for 20 min. Finally, the cell suspension (3 \( \times \) 10\textsuperscript{3} cells/mL) was planted on the substrates at 37°C for 20 min. After washing away the suspending cells with phosphate-buffered saline, the adherent cells were located on the designed patterns. The prepared cell assemblies were incubated at 37°C and 5% CO\textsubscript{2} for 2 h before the two-channel time-lapse snapshot experiments or for 8 h before the Ca\textsuperscript{2+} imaging experiments.

For preparation of fluorescent FN, the FN solution was mixed with a reactive dye (Cy3.5; GE Healthcare, Amersham, UK) for 20 min. Then, the resulting Cy3.5-FN was spread over the substrates. The Cy3.5-FN was excited by a mercury lamp with a 546/12 nm excitation filter, and the corresponding fluorescence emission was collected through a 590/35 nm emission filter.

Imaging

The fluorescence emission associated with calcium concentration in cytosol ([Ca\textsuperscript{2+}]\textsubscript{C}) was detected by an electron multiplying charge-coupled device (DU-897D-CS0-BV; Andor, Belfast, UK) connected to an inverted fluorescent microscope (Axio Observer D1; Carl Zeiss, Oberkochen, Germany). The BV-2 microglial cells were loaded with 2 \( \mu \)M Fluo-4 AM (Invitrogen, Carlsbad, CA) in Hank’s balanced salt solution (137 mM NaCl, 5.3 mM KCl, 2 mM CaCl\textsubscript{2}, 1 mM MgCl\textsubscript{2}, 5.5 mM glucose, 10 mM HEPES (pH 7.4)) for 30 min at 37°C. After bathing in Hank’s balanced salt solution for 10 min, they were excited by a mercury lamp using a 485/0 nm excitation filter. The fluorescence emission was collected by a 40×/1.30 oil objective with a 540/50 nm emission filter. The acquired images were analyzed by MetaMorph software (Molecular Devices, San Jose, CA). Changes of [Ca\textsuperscript{2+}]\textsubscript{C} are presented by modifications of the relative fluorescence intensity FF/Fo (intensity after stimulation/basal intensity before stimulation).

A two-channel time-lapse imaging was performed by using an inverted fluorescent microscope (Ti-E; Nikon, Tokyo, Japan) combined with a CCD (Retiga R1; Qimaging, Surrey, Canada) detector. The images were acquired with Micro-Manager software (National Institutes of Health, Bethesda, MD) at a rate of 1 frame every 3 min.

Mechanical stimulus

A glass microelectrode with a 1-\( \mu \)m-diameter tip fixed on a Three-axis Hanging Joystick Oil Hydraulic Micromanipulator (MMD-202ND; Narishige, Tokyo, Japan) was used to mechanically stimulate single BV-2 microglial cells. The tip was manipulated to provoke a gentle stimulation on the membrane of a selected micropatterned cell.

Statistical analysis

When a selected cell exhibited a rise of [Ca\textsuperscript{2+}]\textsubscript{C} resulting in \((F_{\text{max}}/F_0) > 1.1\), it was regarded as a Ca\textsuperscript{2+}-responsive cell. The response ratio is defined as the number of responsive intercellular-bridge-connected cells divided by the total number of all intercellular-bridge-connected cells in the investigated group. The response intensity is defined as the fluorescence intensity of the Ca\textsuperscript{2+} signal in the stimulated state divided by the fluorescence intensity in the resting state. The length of the intercellular bridge is defined as the length of the connecting tissue that has a width of less than 2 \( \mu \)m. The abscission time is defined.
as the time interval between the moment at which the cell was divided into two cells and the moment at which the intercellular bridge was terminated. The obtained data are presented as the mean ± standard deviation (SD). For statistical comparison between different groups, the data were analyzed by GraphPad Prism software (version 6) using an unpaired Student’s t-test. The values of \( p < 0.05 \) were considered to be statistically significant.

RESULTS

Propagation of \( \text{Ca}^{2+} \) waves between BV-2 microglial cells connected with intercellular bridges

First, BV-2 microglial cells cultured on traditional substrates were investigated. They formed intercellular bridges during the cell division (Fig. 1A). The immunostaining experiment demonstrated that the intercellular bridges were composed of microtubular bundles with a characteristic midbody structure located in the middle of the intercellular bridge (Fig. S1A). Although some intercellular bridges were as long as 30 \( \mu \text{m} \), most of them were shorter than 5 \( \mu \text{m} \) (Fig. S1B). Before applying the mechanical stimulus (Fig. 1A), all cells were in the resting state according to the stable basal [\( \text{Ca}^{2+} \)]_c (F/F_0 = 1 in Fig. 1B). As can be seen in Fig. 1 and Video S1, a gentle touch of the microelectrode evoked a rapid increase of [\( \text{Ca}^{2+} \)]_c in cell 1, followed by propagation of the signal through the intercellular bridge and mobilization of [\( \text{Ca}^{2+} \)]_c in the body of cell 2. This observation demonstrates that intercellular bridges are capable of mediating \( \text{Ca}^{2+} \) communication. Interestingly, cell 3, which was physically separated from cells 1 and 2, also exhibited an increase of [\( \text{Ca}^{2+} \)]_c. This increase was stimulated through the paracrine pathway. As demonstrated in our previous work, the transmitters mediating the \( \text{Ca}^{2+} \) communication are secreted from the stimulated site on cell 1 (marked by an asterisk in Fig. 1A) was almost equidistant from cell 2 and cell 3, whereas the increase of [\( \text{Ca}^{2+} \)]_c in cell 2 appeared much faster than in cell 3 (Fig. 1B). This result suggests that \( \text{Ca}^{2+} \) communication mediated by the intercellular bridge is considerably faster than \( \text{Ca}^{2+} \) communication mediated by the paracrine pathway.

To resolve additional details on the spatiotemporal characteristics of the \( \text{Ca}^{2+} \) communication mediated by the intercellular bridge, we developed a simple micropatterning strategy to induce longer intercellular bridges. This strategy was motivated by the expectation that measurements of \( \text{Ca}^{2+} \) propagation velocities would be more precise on longer intercellular bridges. Moreover, with a predesigned bridging location, the mechanical stimulus can be always applied at one and the same site of the stimulated cells.

Regulation of intercellular bridges with micropatterned assemblies

To induce longer intercellular bridges between BV-2 microglial cells, we designed a set of dumbbell-shaped micropatterns. Circular parts of the patterns had a diameter of 18 \( \mu \text{m} \) (Fig. 2A), which corresponds to the typical size of BV-2 microglial cells cultured on traditional substrates. A bar connecting the two circular ends had a width of 6 \( \mu \text{m} \) and lengths in the range from 2 to 30 \( \mu \text{m} \). The fluorescence distribution of Cy3.5-FN deposited onto such a pattern is also shown in Fig. 2A and reveals that the FN area is consistent with the designed pattern. When single BV-2 microglial cells were cultured on the substrates, they adhered to one of the two circular regions, as shown in Fig. 2B. Then, the cell divided into two daughter cells that moved away from each other and formed an intercellular bridge between them. The bridge was located on top of the connecting bar of the dumbbell-shaped micropattern (Fig. 2B; Video S2). To select optimal micropatterns for the following \( \text{Ca}^{2+} \) imaging experiments, we performed statistical analysis of the maximal observed length (before final abscission) of the intercellular

![FIGURE 1](image_url) Ca\(^{2+}\) communication among BV-2 microglial cells. (A) A sequential series of pseudocolor fluorescence images of Ca\(^{2+}\) communication between the cells is given. The signal was elicited by a mechanical stimulus (glass electrode) applied to cell 1. The asterisk indicates the stimulated site. Cells 1 and 2 are connected with an intercellular bridge. The white arrow indicates the location of the midbody of the intercellular bridge. Scale bar, 10 \( \mu \text{m} \). (B) The [Ca\(^{2+}\)]_c traces of the three cells shown in (A) are shown. The Ca\(^{2+}\) mobilization in cell 2 is significantly faster than in cell 3. To see this figure in color, go online.
bridge as a function of the length of the connecting bar. As shown in Fig. 2C, the lengths of intercellular bridges were 2.7 ± 0.8, 5.7 ± 1.8, 6.7 ± 1.5, 8.7 ± 2.7, 9.8 ± 2.2, 16.3 ± 5.6, and 24.5 ± 7.8 μm for the bars with lengths of 2, 4, 6, 8, 10, 20, and 30 μm, respectively. One can notice that for bars shorter than 10 μm, the average length of the resultant intercellular bridges is longer than the length of the bars, whereas for bars longer than 10 μm, it is shorter. Fig. 2D shows the corresponding values of the abscission times, which are 113 ± 22, 115 ± 26, 137 ± 23, 169 ± 22, 165 ± 31, 157 ± 31, and 143 ± 34 min. In general, the abscission time increases with increasing length, indicating that longer intercellular bridges are more stable than the short ones. In accordance with this finding, we chose a pattern with bar lengths of 8, 10, 20, and 30 μm for further experiments. We also found that the response ratios and the response intensities decreased slightly as the bar lengths of the pattern increased from 8 to 30 μm (Fig. S2). This might be because longer intercellular bridges are often narrower, which impedes intercellular transmission.

**Passive Ca²⁺ diffusion and endogenous Ca²⁺ response contribute to increase of \([\text{Ca}^{2+}]_c\) in the connected cell**

We recorded modifications of \([\text{Ca}^{2+}]_c\) as a function of time after mechanical stimulation of one of the two connected cells. A typical result presented in the form of a kymograph image is shown in Fig. 3A (see also Video S3). The cell on the right side was stimulated first. Afterwards, a weak passive Ca²⁺ diffusion propagating from the stimulated cell to the midbody of the intercellular bridge and then to the opposite end of the bridge was detected. The evolution of this signal is indicated in Fig. 3A by the dashed line K2. Then, an endogenous Ca²⁺ response took place in the connected cell (Fig. 3A; Video S3). The corresponding signal was much larger than the signal from passive Ca²⁺ diffusion and emanated from the central part of the cell body of connected cell rather than from the joint between the connected cell and the intercellular bridge. This observation indicates an indirect pathway of the \([\text{Ca}^{2+}]_c\) increase in the connected cell. The evolution of this signal is indicated in Fig. 3A by the dashed line K1. Quantitative statistical analysis of the slopes of K1 and K2 is presented in Fig. 3B. The slope of K2 (9.7 ± 2.7 μm/s) corresponds to an effective transit velocity of passive Ca²⁺ diffusion along the intercellular bridge. The slope of K1 (6.6 ± 2.0 μm/s) corresponds to an effective propagation velocity of the endogenous Ca²⁺ signal. From those observations it follows that both passive Ca²⁺ diffusion and endogenous Ca²⁺ response contribute to the increase of \([\text{Ca}^{2+}]_c\) in intercellular-bridge-connected cells. The former is faster but quite weak, whereas the latter is slower but much stronger.
Transmission of IP₃ via intercellular bridge mediates endogenous Ca²⁺ response in the connected cell

To elucidate the source of endogenous Ca²⁺ response, various reagents were applied to the cells before mechanical stimulation. Fig. 4 shows the corresponding response ratios and response intensities of the associated endogenous Ca²⁺ signal. The results show Ca²⁺-free medium treatment had no impact on signal propagation, indicating its independence from extracellular Ca²⁺. Our previous work showed that pretreatment with ATP (10 μM) could terminate Ca²⁺ communication mediated by the paracrine (30,31). In this work, pretreatment with 10 μM ATP had almost no effect, which indicates that for intercellular-bridge-mediated Ca²⁺ communication, the paracrine pathway is practically negligible. Moreover, a similar result was obtained when cells were pretreated with MRS 2211 (10 μM, 15 min), a P2Y₁₃ receptor-specific inhibitor that could block the paracrine-mediated intercellular Ca²⁺ communication in BV-2 microglia (31).

The cells were also pretreated with application of endoplasmic reticulum Ca²⁺-ATPase inhibitor thapsigargin (TG) (32) and IP₃ receptor blocker 2-aminoethyl diphenylborate (2-APB) (33). The preincubation took place for 10 min at room temperature with either 2 μM TG or with 15 μM 2-APB. Both of those reagents significantly decreased the response ratios (Fig. 4 A) and the response intensities (Fig. 4 B) of Ca²⁺ in the connected cell, suggesting that the main source of intercellular-bridge-mediated endogenous Ca²⁺ response is IP₃-sensitive calcium store release.

In contrast to endogenous Ca²⁺ response, passive Ca²⁺ diffusion into the connected cells was clearly observed even when the endogenous Ca²⁺ response was inhibited by the 2-APB (arrows in Fig. 5 A; Video S4). In this case, a slight increase of Ca²⁺ fluorescence initiated from the end of the intercellular bridge was detected without a subsequent endogenous Ca²⁺ increase in the connected cell. The traces represented in Fig. 5 B show that Ca²⁺ flowed into the intercellular bridge practically immediately after the [Ca²⁺]c increase in the stimulated cell, whereas a significantly weaker Ca²⁺ increase occurred in the connected cell. On the other hand, we applied BAPTA-AM (10 μM, 20 min), a potent free Ca²⁺ chelator, to further study intercellular bridge-mediated Ca²⁺ signals. The results showed that Ca²⁺ diffusion fluorescence was completely suppressed, whereas IP₃-mediated Ca²⁺ release
fluorescence just decreased evidently (Fig. S3; Video S5). The Ca\(^{2+}\) dissociation constants are \(~345\) and \(~700\) nM for fluo-4 (34) and BAPTA (35), respectively, suggesting that BAPTA binds free Ca\(^{2+}\) more easily than fluo-4. Thus, the large majority of the released Ca\(^{2+}\) was chelated by BAPTA after IP\(_3\) activated calcium stores in the connected cell, which resulted in a small increase of Ca\(^{2+}\) fluorescence (orange line in Fig. S3 B). Meanwhile, the Ca\(^{2+}\) diffusion fluorescence through the intercellular bridge was totally blocked because of the BAPTA chelation (green line in Fig. S3 B). According to these results, we believe that intercellular communication via direct Ca\(^{2+}\) diffusion is also important for cell-cell communication between intercellular-bridge-connected cells.

### Simulation of Ca\(^{2+}\) and IP\(_3\) diffusion through the intercellular bridge

To verify the possibility that passive Ca\(^{2+}\) diffusion along the intercellular bridge can increase \([\text{Ca}^{2+}]_c\) level in the connected cell, we simulated Ca\(^{2+}\) diffusion between two cells connected by intercellular bridges using the model previously described (28) (Supporting Materials and Methods). Results show that passive diffusion of Ca\(^{2+}\) raises calcium concentration in the intercellular bridge (\([\text{Ca}^{2+}]_b\)) (Fig. 6 A) as well as in the connected cell (\([\text{Ca}^{2+}]_c\)) (Fig. 6 B), in good accordance with the experimental results shown in Fig. 5.

Previous work reported that Ca\(^{2+}\) diffusion in cytoplasm was much slower than IP\(_3\) diffusion because Ca\(^{2+}\) buffer in cytoplasm could bind to Ca\(^{2+}\) ions and slow their motion (36). However, in our system, the IP\(_3\)-mediated Ca\(^{2+}\) response in the connected cell was slower than the passive Ca\(^{2+}\)-diffusion-mediated response (Fig. 3). After the application of mechanical stimulus, the concentrations of both Ca\(^{2+}\) and of IP\(_3\) increased in the stimulated cell. Subsequently, their diffusion through the intercellular bridge toward the connected cell took place. As reported in (37,38), IP\(_3\) in the connected cell should reach a threshold concentration of \(~0.5\) \(\mu\text{M}\) to be able to induce an endogenous Ca\(^{2+}\) release. As can be seen in Fig. 6 D, in our system, this causes a delay of some seconds, which in our opinion explains why in intercellular-bridge-connected cells, endogenous Ca\(^{2+}\)-response-based signaling is slower than passive Ca\(^{2+}\)-diffusion-based signaling.

### DISCUSSION

The increase of Ca\(^{2+}\) level in cytosol plays a crucial role in various processes during cell division such as activation of Aurora-A kinase at mitosis (39), modulation of spindle formation and the onset of anaphase (40), and induction of calmodulin-dependent protein kinase II, which triggers the exit from meiosis (41). Our results clearly demonstrate that intercellular bridges mediate the cytosol Ca\(^{2+}\) levels via two different pathways, which brings a new perspective to the general understanding of Ca\(^{2+}\) regulation during mitosis.

TNTs, a tube-like continuity in plasma membrane and cytoplasm of adjacent cells, are formed by protrusion of filopodia or the separation of contacted cells with a length of tens of micrometers and a width of 50–200 nm (42). They allow intercellular transmission of multiple types of cellular components such as proteins, RNAs, viruses, and organelles (43,44). It has been established how TNTs facilitate Ca\(^{2+}\) signaling between isolated cells and that the diffusion of IP\(_3\) along the TNTs and IP\(_3\)-mediated Ca\(^{2+}\) liberation promote the propagation of Ca\(^{2+}\) signals through them (28,29). Our observations indicate that, similar to TNTs, intercellular bridges also predominantly facilitate the IP\(_3\)-mediated Ca\(^{2+}\) liberation. However, because intercellular bridges are relatively wide in comparison to TNTs, passive diffusion of Ca\(^{2+}\) through them can also induce the raise of \([\text{Ca}^{2+}]_c\) in the connected cells. In accordance with that assumption, we carried out numerical simulations by using a model developed for TNTs (28) but considering a larger radius (\(~1\) \(\mu\text{m}\) instead of \(~200\) nm) of the connecting tubes. The obtained results are in good agreement with the experimental data.
accordance with experimental observations. Another intercellular linkage, gap junction channels, are composed of two end-to-end hemichannels, each of which contains six connexin subunits surrounding the central pore (~40 Å in diameter) (45). Gap junctions can also mediate communication between closely contacted cells by facilitating the exchange of small molecules and ions (46). It has been reported that gap junctions mediate the intercellular Ca\(^{2+}\) signaling through the diffusion of Ca\(^{2+}\) and IP\(_3\)-mediated Ca\(^{2+}\) release (47), which is similar to our results on the intercellular-bridge-mediated Ca\(^{2+}\) communication.

Our work also provides an appealing demonstration of the versatility of micropatterning as an emerging powerful tool for single-cell control. Recently, micropatterning techniques have been successfully used in investigations of diverse biological processes such as cellular communication (48, 49), migration (50, 51), and cell proliferation and differentiation (52, 53). Our previous study with ring-shaped micropatterned cell assemblies provided experimental evidence of a regenerative amplification mechanism that mediates Ca\(^{2+}\) communication between physically isolated BV-2 microglial cells via the paracrine pathway (30). In this study, dumbbell-shaped micropatterns are used as adhesive islands for control and lengthening of the intercellular bridges between connected cells.

We observed that the abscission time of the intercellular bridge was longer for longer bars. Lafaurie-Janvore et al. obtained a similar result for HeLa cells by using disk-shaped and bar-shaped patterns (7). They further proved that lengthening of the intercellular bridge prevented the assembly of ESCRT-III, which resulted in delayed abscission. When tension along the bridge was released, ESCRT-III assembled and induced membrane fission, followed by abscission. This may also explain why in our experiments, long intercellular bridges have longer lifetimes than shorter ones.

Recently, a cell-cycle-dependent mitochondrial Ca\(^{2+}\) transient was found to coordinate energy production in mitochondria and promote mitotic progression (54). Mitochondria are known to be important sensors, stores, and regulators of Ca\(^{2+}\) (55, 56). Interestingly, in our experiments, by using Mito-Tracker Orange we also observed mitochondria resident in intercellular bridges between the BV-2 microglial cells (Fig. S4). Therefore, we suspect that mitochondria acting as regenerative amplifiers may facilitate also the propagation of Ca\(^{2+}\) waves over the intercellular bridges. Thus, Ca\(^{2+}\) communication mediated by intercellular bridges may regulate formation and abscission processes of cytokinesis through the interaction with mitochondria. Further experiments are needed to analyze the correlation between different processes and verify this proposition.

In summary, we induced long intercellular bridges between BV-2 microglial cells using dumbbell-like micropatterns, by which the spatiotemporal characteristics of mechanical-stimulus-evoked Ca\(^{2+}\) communication through the intercellular bridge were resolved. Ca\(^{2+}\) in the intercellular bridge was observed to transit faster than the responding velocity between intercellular bridge-connected cells. Our results using TG and 2-APB demonstrated that the main source of [Ca\(^{2+}\)]\(_c\) increase in connected cell was passive Ca\(^{2+}\) diffusion and IP\(_3\)-sensitive calcium store release. A theoretical simulation also confirmed the experimental observations. Our work brings a new understanding of Ca\(^{2+}\) signaling mediated by the intercellular bridge during mitosis, as well as proposing an insight into the Ca\(^{2+}\) transmission in narrow bounded structures.
SUPPORTING MATERIAL

Supporting Material can be found online at https://doi.org/10.1016/j.bpj.2020.01.006.

AUTHOR CONTRIBUTIONS

F.X., J.L., and J.Y. performed the experiments. F.X. and S.Q. performed the simulations. F.X. and F.H. analyzed the data. L.P., F.X., and I.D.-O. wrote the article. L.P. and J.X. designed and supervised the work.

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